



## Macromolecular Nanotechnology

## Physical properties of ion beam treated electrospun poly(vinyl alcohol) nanofibers

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## ABSTRACT

We show that the mechanical properties of nano-sized electrospun poly(vinyl alcohol) fibers can be modified using broad-energy ion beam implantation. The elastic moduli were determined using atomic force microscopy multi-point mechanical bending tests on individual fibers before and after treatment. With a dose of  $8.0 \times 10^{15}$  ions/cm<sup>2</sup> of nitrogen ion we observed 30% increases in fiber elastic modulus with a simultaneous fiber diameter reduction. Two additional doses of nitrogen ion as well as a  $8.0 \times 10^{15}$  ions/cm<sup>2</sup> of helium ion treatment showed that this stiffness improvement effect was dependent on ion dosage and ion species. The surface morphological features of the fiber mat were shown to be unaltered due to the ion beam treatment. Key chemical modifications via nitrogen ion treatment were the introduction of the functional groups amine and amide. These groups are important in promoting cell compatibility on polymer surfaces.

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## 1. Introduction

Electrospinning [1] is a simple but versatile technique capable of producing three-dimensional non-woven fiber mats from a wide variety of synthetic and natural polymers [2] including proteins [3] for applications such as membranes [4], wound dressings [5], scaffold for tissue engineering [6] and protective clothing [7]. Electrospun fiber mats, consisting of nanometer sized fibers within a narrow range of fiber diameters, can provide exceptional performance and efficiency in these applications due to their high surface-to-volume ratios and interconnecting porous network. Of particular interest is the development

of scaffolds for tissue engineering. The electrospinning technique is fast becoming the method of choice for their fabrication [8]. In addition, polymer-nanofiber scaffolds can be electrospun with controlled alignment to mimic the natural extracellular matrix [9].

Ion implantation is a well-established technique in the materials post-processing industry, largely because of its controllability and reproducibility. Choosing implantation parameters such as ion species, energy, current and dose allow us to selectively modify tribological [10], chemical [11] and physical properties [12] of a material. For temperature-sensitive polymers, the ability to control these treatment parameters becomes more critical as excessive energy deposition at the surface could cause permanent damage to the material [13,14]. Broad-energy (non-monochromatic) ion beam implantation is often used because, relative to monochromatic beam, it provides a wider range of ion doping depths, thus distributing energy over a greater depth range and minimizing thermal damage [15]. This

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approach is commonly used for improving surface mechanical properties of bulk polymer materials (e.g., for surface hardening [16–18]). For a tissue engineered scaffold, the ability to tailor its stiffness to mimic the natural environment can induce more normal and stable cell adhesion [19,20]. For instance, implantation of helium ions results in drastic alteration of the cell adhesion properties of polypropylene and polytetrafluoroethylene [21]. Incorporating nitrogen via ion beam implantation near the surface of certain synthetic polymer scaffolds can form particular nitrogen-containing functional groups that enhance the attachment of protein and cell [22,23]. Therefore, ion beam treatment can be a convenient method to tailor both the mechanical and chemical properties of polymer surfaces for specific applications. Of particular interest is the potential ability of implanting specific ion species, nitrogen and helium, both of which have been proven to alter cell adhesion properties, to also modify the mechanical properties of polymer fibers.

The purpose of this work is to demonstrate the potential of surface ion beam treatment to modify the mechanical and chemical properties of polymer fibers prepared using electrospinning techniques. A hydrophilic poly(vinyl alcohol) (PVA) polymer is used here because of its good thermal stability, chemical resistance, biocompatibility [24]. Mechanical properties of individual PVA fibers prior to, and following, ion beam treatment were determined using an atomic force microscopy (AFM) multi-point bending test and analysis routine developed in our laboratory [25].

## 2. Experimental methods

### 2.1. PVA fiber production by electrospinning

An electrospinning solution was prepared by dissolving 10.8 wt% of PVA (molecular weight ( $M_w$ ) = 89,000–98,000 g/mol, 99+% hydrolyzed, Sigma–Aldrich) in a solvent consisting of 80% de-ionized water and 20% ethanol. The solution was heated to 50 °C prior to electrospinning. Process parameters used were an electric field gradient of 1.5 kV/cm and solution feed rate of 0.18 ml/h.

For the study of fiber morphology, chemical properties and crystallinity, PVA fibers were collected on an aluminum foil in the form of a randomly orientated non-woven mat. To collect individual, isolated electrospun fibers for AFM mechanical testing, a transmission electron microscopy (TEM) grid (Structure Probe, Inc.) with 7.5  $\mu\text{m}$  square mesh was used on a silicon substrate and mounted at the center of the collector.

### 2.2. Ion beam treatment

Nitrogen ( $\text{N}^+$ ) and helium ( $\text{He}^+$ ) ion beams were generated using the 1.7 MV tandemron accelerator at The University of Western Ontario. Fibers on Al foil or TEM grids (with Si substrate) were mounted on the sample holder with a 1.0  $\mu\text{m}$  thick tantalum (Ta) foil (Ta, 99.9% purity, Goodfellow Cambridge Ltd.) placed to intersect the ion beam 2 mm in front of the sample. The thickness of the foil was confirmed with scanning electron microscope (SEM). Ion beam

treatment was performed with the sample placed vertically at room temperature in ultra-high vacuum ( $\sim 10^{-8}$  torr). The beam currents of  $\text{N}^+$  and  $\text{He}^+$  were limited to 180 nA and 130 nA, respectively.

The simulation software package SRIM-2008 [26] provides theoretical projection of the energies, doping depth profiles and total deposited energy distribution of the two ion species in the PVA fibers after transmission through the foil. Based on the simulated results, the Ta foil reduces the initial ion energies of 1.7 MeV for  $\text{N}^+$  and 520 keV for  $\text{He}^+$  to a suitable broad energy range ( $>0$ –300 keV for  $\text{N}^+$  and  $>0$ –100 keV for  $\text{He}^+$ ) for implantation into the PVA fibers with nearly identical doping depth profiles, ranging from the surface to about 900 nm deep. As expected, the total amount of energy deposited into the sample is then calculated as 3.2 times higher for  $\text{N}^+$ .

The fractions of  $\text{N}^+$  and  $\text{He}^+$  beam that penetrate the foil and are implanted into the fibers (the total doping yield) are 48% and 53%, respectively. However, all ion implantation doses (in ions/cm<sup>2</sup>) reported in this work are incident doses to the fibers.

### 2.3. Surface characterization of PVA fibers

The suspended length and diameter (suspended portion) of all fibers for AFM measurements were determined from SEM topological images, which were obtained with a Leo 1530 (LEO Electron Microscopy Ltd) at 1 or 2 kV, using the Java-based image processing program, ImageJ (National Institutes of Health). No conductive coating was applied to the samples.

X-ray diffraction (XRD) spectra were collected using a Rigaku-MiniFlex powder diffractometer with a Cu-K $\alpha$  radiation source operating at 30 kV and 15 mA. The  $2\theta$  spectra were scanned from 10.0° to 70.0° with a 0.1° step size.

X-ray photoelectron spectroscopy (XPS) system from Kratos Axis Ultra was used with a 210 W Al-K $\alpha$  monochrome source to analyze the chemical modifications resulting from the ion beam treatments of the fibers. The pass energy of the survey scan was 160 eV and the high-resolution scan was 20 eV. The program CasaXPS (Casa Software Ltd.) was used to construct and curve-fit multiple peaks for the data envelop that appeared in the core-level energy spectra based on the built-in Marquardt–Levenberg [27] optimization algorithm.

### 2.4. Nanomechanical measurements using the AFM

Mechanical testing of individual PVA fibers was performed using a multimode AFM with a Nanoscope IIIa controller (Veeco Instruments) at room temperature with relative humidity between 22% and 35%. Two different triangular silicon nitride cantilevers (NP Series Probes, Veeco Instruments) with nominal spring constants of 0.32 and 0.12 N/m, respectively, were chosen to carry out imaging and mechanical testing of the native unmodified and ion-beam modified fibers. The actual spring constants were determined using the thermal noise technique [28] as  $k_1 = 0.21 \pm 0.01$  N/m and  $k_2 = 0.097 \pm 0.002$  N/m, respectively. These values were periodically confirmed during the experiments.

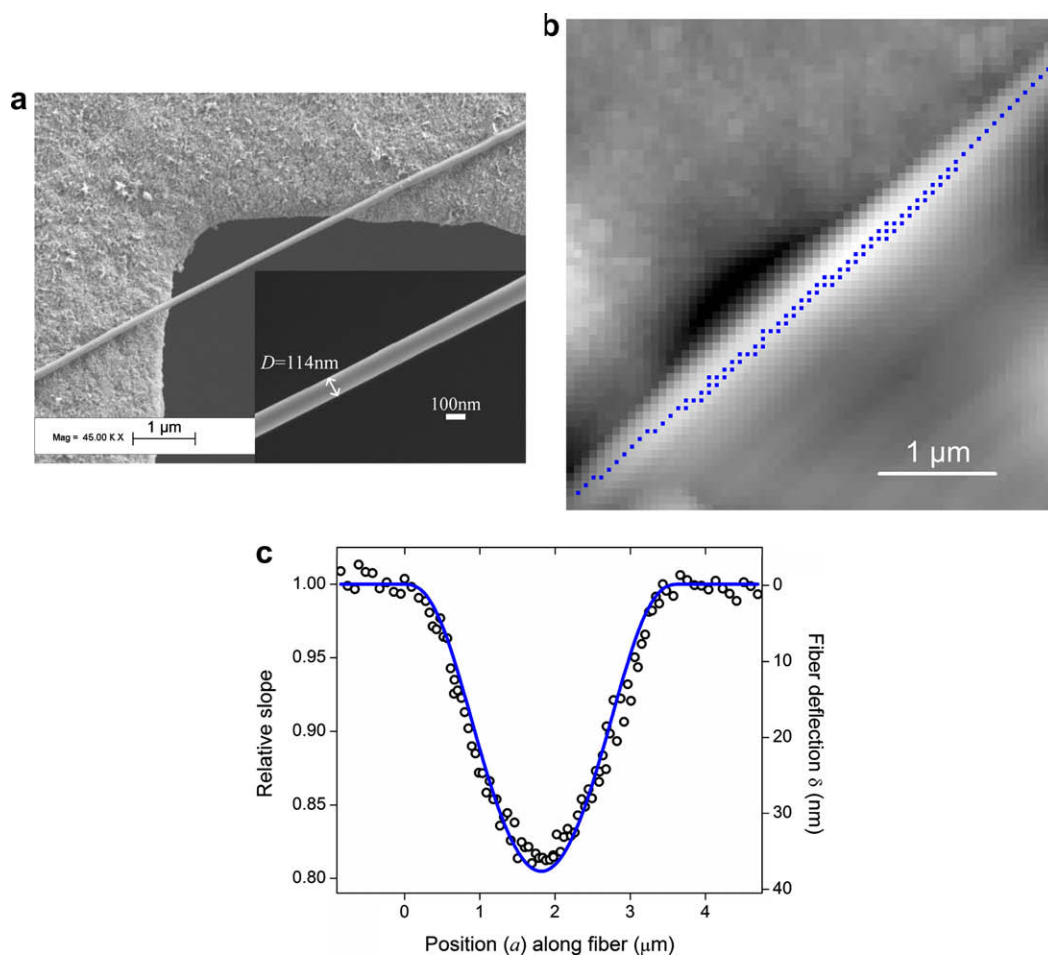
Prior to mechanical testing, optical microscopic images were used to identify the precise location of every suitable fiber on TEM grid. These served as a map for AFM and SEM measurements before and after ion beam treatment. Contact AFM images of the targeted area were used to adjust the scanning position and size to include the entire suspended portion and a sufficient fraction of the supported portion on both ends of each target fiber with a minimal scan size.

Several approaches of AFM-based measurement of mechanical properties of individual fibers have been developed [29,30], but performing a bending test on the suspended section of a clamped fiber in the AFM force–volume mode, as described previously [25], allows the fiber to be examined before and after ion beam treatment. The force spectra with the z-scan size limited at 500 nm were acquired for positions in an array of  $64 \times 64$  pixels spanning square regions of width 3.5–5.0  $\mu\text{m}$  at a z-scan rate of 5 Hz. Another  $64 \times 64$  pixels topographic image is acquired simultaneously by recording the piezo height required to

achieve the trigger threshold corresponding to the maximum force; the maximum force applied to the sample was 37 and 17 nN for the stiffer and softer cantilevers.

We chose 27 fibers with diameters in the range of 106–155 nm and suspended lengths of 3.1–5.6  $\mu\text{m}$  on two separated TEM grids for AFM mechanical testing to investigate the effect of  $\text{N}^+$  and  $\text{He}^+$  treatment. A representative example of such a fiber is shown in the SEM image of Fig. 1a. This range of fiber size allowed all mechanical measurements to be conducted with a single AFM tip under fixed operating parameters in the force–volume mode. The diameter  $D$  of the fiber was determined from a higher resolution SEM image on the suspended portion of the fiber, as shown in the inset of Fig. 1a. We averaged the diameter of 10 locations along the fiber axis. For the fiber shown, the average diameter was  $114 \pm 4$  nm, where a standard deviation of  $\pm 4$  nm was due to the diameter irregularity of the electrospun fiber.

The clamped-beam model was applied to analyze the experimental data. A suspended fiber of length  $L$  is



**Fig. 1.** (a) SEM image of a fiber suspended across a corner of a TEM grid hole. The inset at the lower right shows a high resolution SEM image of the same fiber measuring an average diameter of 114 nm. (b) A topographic image from the AFM force–volume measurement with 92 data points chosen along the fiber. (c) Plot of the slopes of force spectra (hollow circles) as a function of position  $a$  along a suspended fiber of length  $L = 3.7 \mu\text{m}$ . The best-fit using the clamped-beam model is shown as a solid curve.

subjected to an applied force  $F$  caused by an AFM tip, which is applied at a distance  $a$  from one of its ends. The deflection  $\delta(a)$  of the fiber due to tensile deformation follows [31]:

$$\delta(a) = \frac{F}{3EI} \left[ \frac{a(L-a)}{L} \right]^3 \quad (1)$$

where  $E$  is Young's modulus of the fiber and  $I$  is its area moment of inertia.

The force curve is varying with the sample displacement ( $\Delta z$ ), which in turn equals to the sum of the cantilever deflection ( $\Delta y$ ) and the fiber deflection ( $\delta(a)$ ) in the contact regime. The force applied by the AFM cantilever is given by  $F = k\Delta y$ , where  $k$  is the spring constant of the cantilever. The slope of the position along a suspended fiber is predicted as:

$$\frac{dy}{dz} = \left[ 1 + \frac{k}{3EI} \left( \frac{a(L-a)}{L} \right)^3 \right]^{-1} \quad (2)$$

The only variable on the right side of Eq. (2) is Young's modulus of the fiber.  $E$  is determined by fitting this equation to the (normalized) slopes measured as a function of position  $a$  along the fiber using the Levenberg–Marquardt [32] nonlinear least-squares fitting algorithm.

Data was extracted from the force–volume images and analyzed using the Igor Pro software package (Wavemetrics) with a custom analysis routine. The elastic modulus was determined from fits to the data of typically more than 60 force spectra chosen from suspended and supported sections along the fiber in a given force–volume image. To select the data points, a topographic image was used to identify the midline of the fiber, as illustrated in Fig. 1b with 92 data points (this image shows the same fiber as Fig. 1a). Generally 2 points were selected close to the midline along every row of pixels crossing the suspended portion of the fiber. Note that only 1 point was selected on the supported portion, as these points do not enter into the curve-fit and are only used to validate the calibration of the deflection sensitivity.

The slopes of the chosen force spectra and the relative fiber deflections were plotted as a function of position  $a$  from one end of the fiber, as shown in Fig. 1c. The solid line in the figure is a fit to Eq. (2). The agreement between experimental data and the derived curve for a clamped-beam model provides confidence that the experimental AFM multi-point mechanical test data validates the model.

### 3. Results and discussions

#### 3.1. Electrospun PVA fiber diameters

To produce polymer fibers with a particular diameter range, an appropriate set of parameters for the polymer solution and the electrospinning process had to be chosen. We used PVA with  $M_w$  range of 89,000–98,000 g/mol. This value plays a significant role in the physical properties of the polymer solution (viscosity, conductivity and surface tension), and affects the final morphology of individual fibers. The role of the  $M_w$  on the PVA fiber morphology

has been studied in detail by Koski et al. [33]. They showed that medium  $M_w$  (50,000–98,000 g/mol) PVA produces bead-free fibers with circular cross-section at a relatively low solution concentration. We also heated the 10.8 wt% PVA solution to 50 °C prior to the electrospinning process; this can reduce polymer chain entanglement and viscosity, which then decreases the surface tension of the solution. Therefore, it allows us to obtain more fibers in a fixed deposition period with a smaller diameter range compared to the solution in room temperature [34].

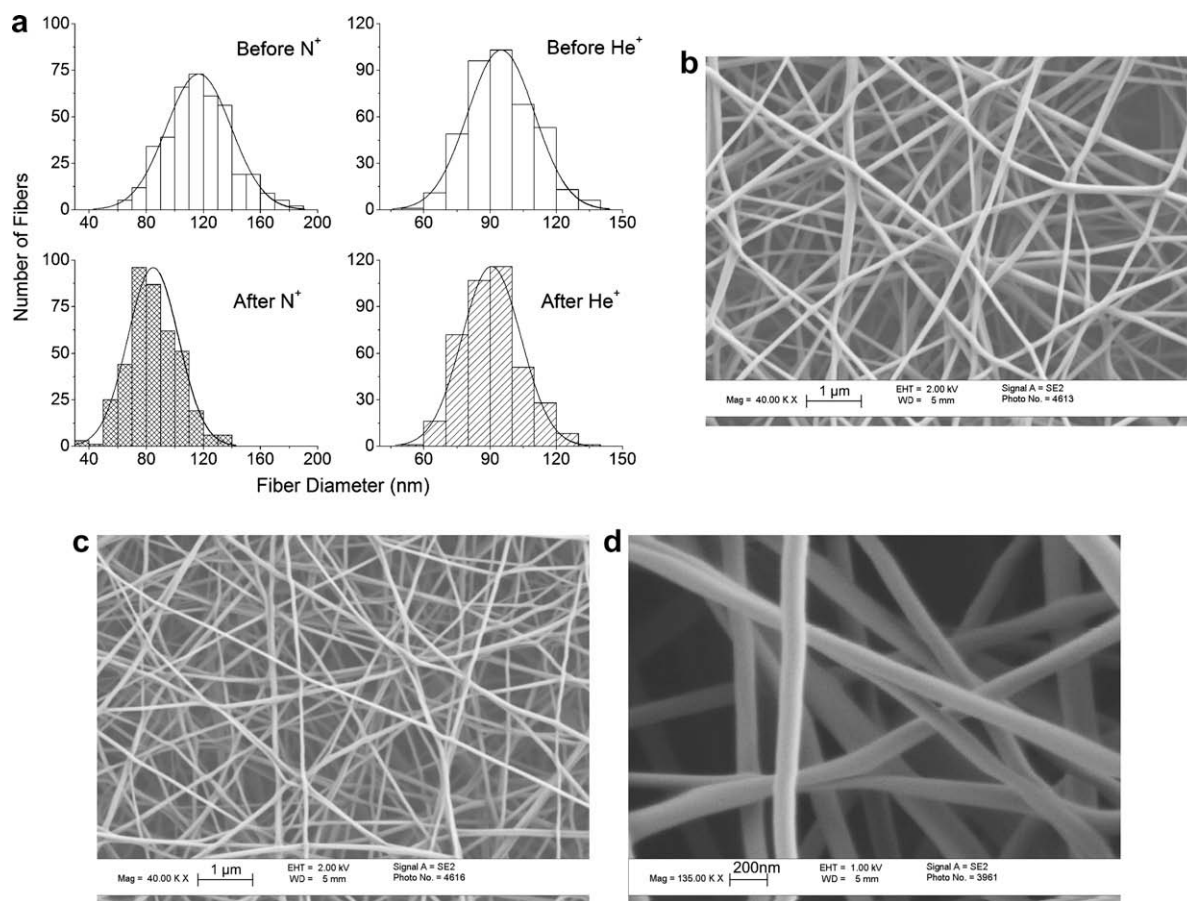
The diameter distribution of a fiber mat was determined from 400 randomly chosen fibers on 10 SEM images captured randomly inside a 4 mm<sup>2</sup> area. The two fiber mats for N<sup>+</sup> and He<sup>+</sup> treatments had original mean diameters of 117 with a standard deviation of 23 nm and 95 ± 15 nm, respectively. The results are shown in the histograms along with best-fit normal distributions in Fig. 2a. One-way ANOVA test showed a significant difference ( $P < 0.01$ ) in the fiber diameter between the two samples. We obtained these two samples using a single 10.8 wt% PVA solution under similar electrospinning conditions, but on two separate days. We attribute this to the only uncontrolled parameters, humidity. Since the PVA solution consisted of 80% of H<sub>2</sub>O, humidity is expected to have a large impact on the evaporation rate of the solvent during the whipping motion of the polymer jet. When the solvent evaporates at a higher rate as would occur in a low humidity environment, the electric field to have less time to stretch the jet into a smaller diameter. On the other hand, high humidity can delay the solidification of polymer jet, which would extend the stretching process to produce smaller fibers. As our result shows that the difference of the fiber diameter caused by the variation of humidity is similar to the study reported by Tripatanasuwan et al. [35].

#### 3.2. Effect of ion beam treatment on fiber diameters

We converted a high-energy mono-energetic ion beam generated from a conventional ion implanter into a low poly-energetic beam using a Ta foil as an energy diffuser. The energy of the beam is reduced and broadened through the collision/straggling process with the Ta atoms before a portion of it is transmitted out of the foil, providing a wide implantation zone [36] in a single process, which in our case covers the range from the surface to 900 nm depth (theoretical SRIM value) of a PVA fiber mat. Using a mono-energetic beam we would need multiple-energy implantation steps to achieve a similar range. Furthermore, the ion energy deposition profile has also been extended into a wider range, minimizing energy-related damage, particularly near the surface.

The high atomic mass of Ta can reduce, but not completely eliminate, the probability of recoil and/or sputtering of foil atoms to the sample. Indeed, the XPS data in later section showed that the surface of nitrogen treated PVA fiber mats contained a significant amount of Ta atoms, which could not be ignored if the treatment was for biomaterials application. However, Ta has long been used as a contrast agent in X-ray imaging and a material in orthopedic implants, and shows cell compatibility [37,38] and no systemic toxicity inside body fluids [39], the presence of





**Fig. 2.** (a) Histograms of the fiber diameter before and after  $N^+$  and  $He^+$  treatment. (b) SEM image of the original PVA fiber mat prior to ion beam treatment. (c) SEM image of the PVA fiber mat after treatment with  $N^+$  dose of  $1.2 \times 10^{16}$  ions/cm<sup>2</sup>. (d) High resolution SEM image of the PVA fibers after treatment with  $N^+$  dose of  $1.2 \times 10^{16}$  ions/cm<sup>2</sup>.

Ta is not expected to diminish the potential of applying this surface treatment technique to any suitable material for biomedical applications.

Fig. 2b shows SEM topological image of the PVA non-woven fiber mat with diameter of  $117 \pm 23$  nm before  $N^+$  treatment. Fig. 2c shows SEM topological image of the same fiber mat after exposure to  $1.2 \times 10^{16}$  ions/cm<sup>2</sup> of  $N^+$ . Visual comparison between Fig. 2b and c indicate that fiber diameter is reduced after ion beam treatment, which also alters the porosity and surface area to volume ratio of the mat, but the bulk porosity is expected to remain unchanged due to the relatively shallow ( $\sim 900$  nm) ion implantation range. Histogram of fiber diameter for the sample after  $N^+$  treatment is shown in Fig. 2a. The treatment resulted in a significant reduction (one-way ANOVA;  $P < 0.01$ ) in fiber diameter of 27% to  $85 \pm 18$  nm, with a reduced diameter distribution from an original range of 63–182 to 40–140 nm. This may be attributed to an ion beam induced annealing effect [40] from the  $N^+$  beam, the kinetic energy of the ions deposited in the fiber with a fraction converting to thermal energy. During the chain scission and cross-linking process, the thermal energy may allow the polymer chains to become mobile and re-arrange their orientations to minimize free space present in the original

structure. Fig. 2d shows a high resolution SEM image of fibers with the same dose of  $N^+$  treatment, in this image no damage to the cylindrical structure of individual fibers nor to the non-woven surface morphology of the mat is apparent.

In parallel, the second PVA non-woven fiber mat was analyzed before  $He^+$  treatment. The surface morphology of this sample was nearly identical to that of equivalent to Fig. 2b, but diameter distribution had a slightly lower mean value of  $95 \pm 15$  nm before ion beam exposure. After exposure to  $1.2 \times 10^{16}$  ions/cm<sup>2</sup> of  $He^+$ , no effect on the fiber diameter was observed with a final diameter of  $91 \pm 13$  nm. With 3.2 times less energy deposited than the  $N^+$  beam, the fibers at the surface encounter less internal annealing process and lead to no significant diameter shrinkage from the  $He^+$  beam. The fiber diameter histogram for the sample after  $He^+$  treatment is shown in Fig. 2a.

In contrast, our previous work, which used a mono-energetic oxygen ion beam [13], resulted in modification that was mostly destructive for polyurethane fibers. The highly localized energy deposition from a monochromatic low energy ion beam can also induce major carbonization [10,14] and melting [13] at the surface of polymeric

materials. Similar irreversible surface morphological damages are also expected from using plasma-based ion implantation systems. Although plasma-based ion implantation is frequently used to vary the original properties and/or introduce new features for particular applications [22,41–43], its high rate of destructive surface sputtering (surface erosion) does not permit treatment of polymeric materials with valuable nano-sized physical features on the surface.

### 3.3. $N^+$ treated PVA fibers and effect of ion dosage

We used the same AFM force–volume mode protocol to measure the same fibers at the same locations before and after ion beam treatment to determine its effect on the elastic moduli of individual fibers. The Young's moduli of 10 fibers were first found to have an original mean value of  $30 \pm 5$  GPa, where the uncertainty is the standard deviation of the 10 fibers. We found good reproducibility and consistency of these results by further repeating the measurements on randomly selected fibers.

Those fibers were then exposed to  $8.0 \times 10^{15}$  ions/cm<sup>2</sup> of  $N^+$  under the conditions (including beam current) described in Section 2.2. We lowered the dose to two-thirds of the value applied to the non-woven mat to reduce the decrease in fiber diameter we observed in previous Section 3.2. This was necessary to maintain a large enough diameter for AFM measurements using the same settings with the same cantilever.

The result from the first  $N^+$  treatment showed an increase in elastic modulus for all 10 fibers, with the average increasing from  $30 \pm 5$  to  $39 \pm 5$  GPa (one-way ANOVA; significant with  $P = 0.01$ ). The mean diameter decreased (one-way ANOVA; significant with  $P < 0.01$ ) from 122 to 108 nm with a standard deviation of  $\pm 8$  nm. Fig. 3a and b summarizes the results of mechanical testing results and the average fiber diameter of the 10 fibers, respectively. It is important to note in this context that based on our AFM contact mode images the shrinkage of the diameter did not affect the clamping condition of the fibers on the TEM grid. This was later confirmed for the rest of the ion beam treatments. Therefore, the clamped-beam model remained valid for determining the elastic modulus of the fibers from the AFM force–volume data.

The next dose step of  $8.0 \times 10^{15}$  ions/cm<sup>2</sup> of  $N^+$  resulted in the apparent onset of a transition stage with two classes of results. For eight of the 10 fibers, we observed a further 10% increase of the elastic modulus to  $43 \pm 5$  GPa (excluding the results of the other two). On the other hand, two fibers experienced  $\sim 36\%$  drop from their original values. These two fibers maintained the same diameter as measured after the first treatment. If we summarize the results of all 10 fibers we find the same value as after the first treatment with a mean elastic modulus of  $39 \pm 11$  GPa and a mean diameter of  $110 \pm 8$  nm, the higher uncertainties in the elastic modulus due to the two deviating fibers. The modifications in elastic modulus and diameter were both significantly different (one-way ANOVA;  $P < 0.01$ ) from the original values, but insignificantly different (one-way ANOVA;  $P > 0.05$ ) from the values after the first treatment.

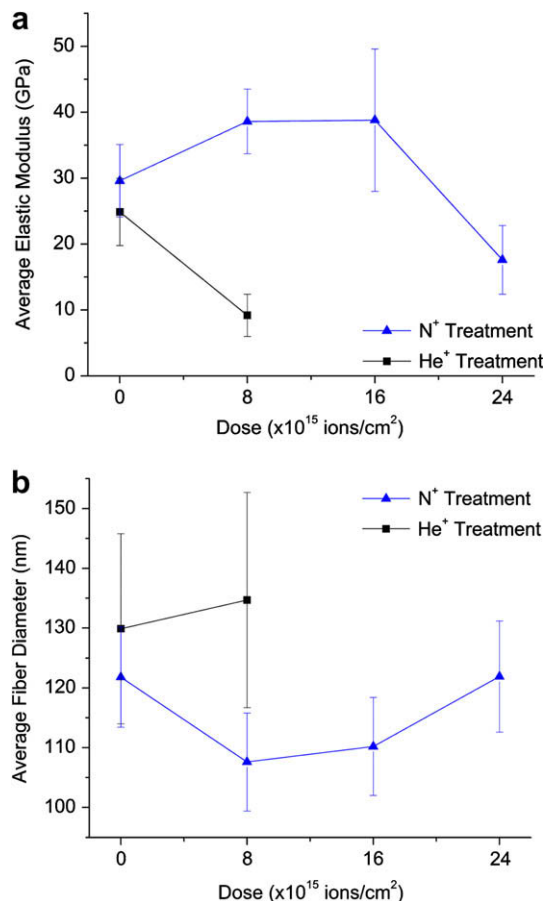


Fig. 3. (a) The average elastic modulus, and (b) the average fiber diameter of the fibers before and after each step of nitrogen ion treatments (triangle) and helium ion treatment (square).

The last step of  $N^+$  treatment then showed the expected result for an overdosed polymer that began to carbonize. All 10 fibers showed weakening to a mean elastic modulus of  $18 \pm 7$  GPa, which is significantly (one-way ANOVA;  $P < 0.01$ ) 54% and 40% drop from the first two treatments and initial mean value, respectively. The mean diameter of the 10 fibers increased to a value of  $122 \pm 9$  nm, which matches the original value.

We measured the PVA fibers with a small diameter range from 100 to 160 nm for two major reasons. First, this can minimize any variation of the elastic modulus with diameter as has been reported for polymer fibers on the nanometer scale [44,45]. Additionally, the stiffness of these fibers all fall within the operational range of a single cantilever, which allows us to perform the mechanical tests on all pre-treated (as well as all post- $N^+$  treated) fibers with a single set of force–volume mode parameters (such as trigger threshold and z-scan size). This avoids any need for extra calibration steps and equalizes the instrumental uncertainty for all fibers. Moreover, the small diameter range minimizes variations in the ion implantation profiles [13] that would occur for fibers of different diameters.

The results indicate that  $N^+$  treatment results in an overall increase in stiffness of the PVA fibers up to a certain total ion dosage ( $1.6 \times 10^{16}$  ions/cm<sup>2</sup>). This stiffness increase can be attributed to the creation of three-dimensional cross-linked polymer chain networks (solubility results shown in Fig. 5) via ion–polymer interaction that results in chain scission, cross-linking, doping and annealing. In addition, there is an incorporation of nitrogen functionalities into the fibers (XPS results shown in Fig. 4), a change in crystallinity (Fig. 6) and a decrease in fiber diameter with a concomitant increase in density (fiber diameter results shown in Fig. 2). All these factors combined are likely led to the observed stiffness increase of the  $N^+$  treated PVA fibers.

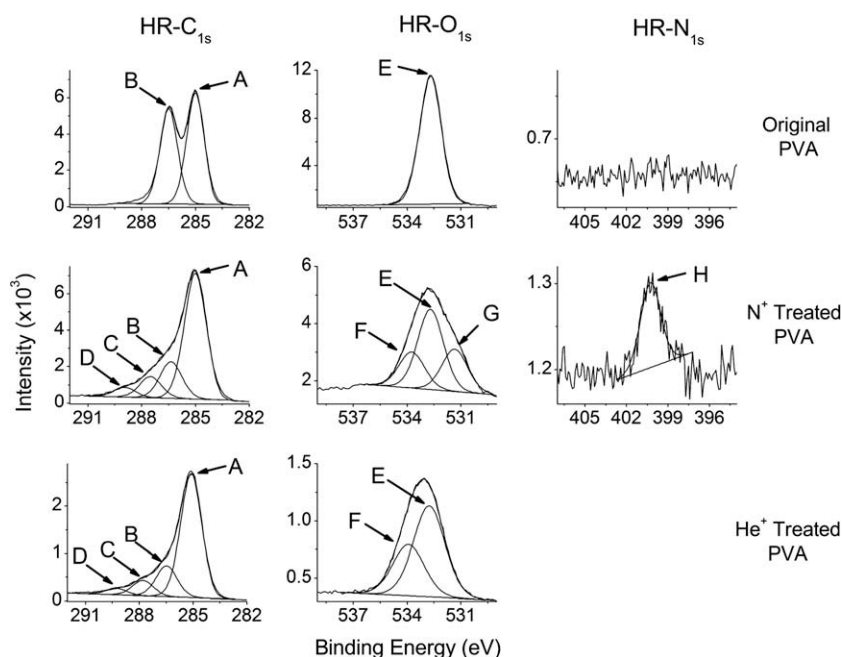
### 3.4. $He^+$ treated PVA fibers

Seventeen PVA fibers deposited on another TEM grid were treated with a single dose of  $8.0 \times 10^{15}$  ions/cm<sup>2</sup> of  $He^+$ . Their elastic moduli were reduced so drastically that an AFM cantilever of smaller spring constant (0.097 N/m) was required to obtain reliable force spectra after the treatment. The elastic modulus of the 17 fibers before the treatment had a mean value of  $24 \pm 5$  GPa with a mean diameter of  $130 \pm 16$  nm. After the  $He^+$  treatment, the elastic modulus dropped dramatically (one-way ANOVA;  $P < 0.01$ ) by about 63% to  $9 \pm 3$  GPa while the diameter remained at  $135 \pm 18$  nm; we thus did not continue helium ion beam treatment. Fig. 3a and b shows the results of the 17 fibers before and after this treatment.

### 3.5. Effect of ion beam treatment on chemical structure

Chemical composition of the PVA fiber mat was analyzed using XPS. It showed the chemical composition of standard PVA [46] with  $71 \pm 1\%$  carbon and  $29 \pm 1\%$  oxygen in the survey spectrum. This baseline can allow us to follow the degree of carbonization induced by the broad-energy ion beam surface treatment on the fibers due to incremental ion dose steps. The first  $8.0 \times 10^{15}$  ions/cm<sup>2</sup> of  $N^+$  increased the proportion of carbon to  $79.3 \pm 0.2\%$  and decreased oxygen to  $20.0 \pm 0.3\%$ . The carbonization effect continued in the same trend for the second dose step and finally reached  $87.2 \pm 0.5\%$  of carbon with  $10.3 \pm 0.1\%$  of oxygen after the third (last)  $N^+$  dose step. On the other hand, despite  $He^+$  transferring a lower amount of energy, the carbonization effect induced by the first  $8.0 \times 10^{15}$  ions/cm<sup>2</sup> of  $He^+$  matches that for the third  $N^+$  dose with relative concentration of  $86.7 \pm 0.5\%$  and  $13.3 \pm 0.1\%$  of carbon and oxygen, respectively. A second  $He^+$  dose was applied and did not further increase the concentration of carbon significantly, which remained at  $87.2 \pm 0.5\%$ .

XPS survey spectra were also used to partially confirm the simulated doping profile of the transmitted ion beam we obtained from SRIM (Section 2.2). The relative concentration of the nitrogen started at  $0.45 \pm 0.02\%$  for the first nitrogen dose step and reached a maximum of  $2.0 \pm 0.5\%$  for the last step. No nitrogen was found in the  $He^+$  treated sample, as expected. As helium is undetectable in XPS measurements, the amount of helium remaining in the sample after the ion implantation process is



**Fig. 4.** High resolution XPS spectra for C<sub>1s</sub> (left column), O<sub>1s</sub> (middle column) and N<sub>1s</sub> (right column), measure for untreated (top row),  $N^+$  treated (middle row) and  $He^+$  (bottom row) PVA fiber mats. The peaks are interpreted on terms of contributions from various chemical groups (lettered peaks), as defined in Table 1.

indeterminable. However, since helium is non-reactive and has a high diffusion coefficient, we expect the amount remaining in the treated sample to be negligible.

The use of Ta foil as an energy diffuser results in the incorporation of this element. XPS data confirmed the presence of Ta in all treated samples, with amounts ranging from 0.15% for the He<sup>+</sup> treated samples to 0.3–0.7% for the N<sup>+</sup> treated samples.

To test for modification of the chemical structure caused by ion implantation, high resolution (HR) XPS spectra of C<sub>1s</sub>, O<sub>1s</sub> and N<sub>1s</sub> were obtained. Fig. 4 shows the HR XPS spectra of C<sub>1s</sub> (1st column), O<sub>1s</sub> (2nd column) and N<sub>1s</sub> (3rd column) for the original PVA fiber mat (top row), as well as the N<sup>+</sup> (middle row) and He<sup>+</sup> (bottom row) implanted samples. The binding energy of each peak was used to determine the corresponding chemical functional groups in the sample. Every peak was labeled alphabetically as shown in Fig. 4. Table 1 provides the list of functional groups registered for each peak with the corresponding binding energy. The C<sub>1s</sub> and O<sub>1s</sub> spectra for the untreated PVA fiber mat matched standard PVA in the database [46]. The curve-fitted peak A and B in the C<sub>1s</sub> spectrum were 53.4 ± 0.6% and 46.6 ± 0.6%, respectively. In this case, the functional group C—OH (alcohol) was the only signal to generate peak B as well as the peak E (100%) in the O<sub>1s</sub> spectrum.

After N<sup>+</sup> treatment, the most obvious change was a new peak H (100%) created in the N<sub>1s</sub> spectrum. This confirmed that implantation of the reactive ions results in chemical reactions. New groups include a reaction with carbon in PVA to form C—N groups (amine and/or amide). In the O<sub>1s</sub> spectrum, two new peaks (F and G) occurred after the N<sup>+</sup> implantation. Peak G with a binding energy of 399.9 eV corresponds to the N—C=O (amide) group. Combining the results with the N<sub>1s</sub> spectrum allows us to confirm the formation of an amide group via N<sup>+</sup> implantation. Furthermore, the percentage of peak G in the O<sub>1s</sub> spectra increased with N<sup>+</sup> dose, starting from 21 ± 2% for the first dose step, increasing to 31 ± 1% after the second step, reaching 35.8 ± 0.2% for the last step. This showed a strong correlation between the trend of the relative concentration and the dose of N<sup>+</sup> implanted in the sample.

C<sub>1s</sub> spectra evolved almost identically for N<sup>+</sup> and He<sup>+</sup> treatment with two new peaks (C and D) supplementing the two original peaks (A and B), as shown in Fig. 4. Since peak C has the same binding energy as the carbon in the amide group, the designation of peak C in the N<sup>+</sup> implanted

sample appeared obvious. However, the observation of the same peak C for the He<sup>+</sup> implantation proved this peak is not exclusive to an amide group. In fact, peak C can also be due to the oxygen-containing hydrocarbon group O—C—O. This observation explains the trend of the percentage of peak C, which started at 11.1 ± 0.2% after the first N<sup>+</sup> dose and decreased to 4.2 ± 0.1% with the last dose. As the O<sub>1s</sub> spectra shows, the number of amide groups indeed increased steadily with the N<sup>+</sup> dose, but the overall number of oxygen atoms dropped as the dose is increased. As more and more oxygen atoms had been recoiled away from the N<sup>+</sup> straggling path, the implantation process changed from creating O—C—O groups to eliminating them. Peak C has a percentage of 8.7 ± 0.1% after the first He<sup>+</sup> dose, and then remains at 10 ± 0.1% after the second dose.

The new peak D, with a binding energy at the high-end of the C<sub>1s</sub> data envelope, belongs to the carbon in the carbonyl part of C—O—C=O (carboxylic ester) group, where the other carbon appears within peak B. Peak D shows a trend similar to that of peak C: beginning at 5.5 ± 0.2% after the first dose of N<sup>+</sup>, then down to 3.0 ± 0.1% with the third dose. For the He<sup>+</sup> treated sample, the carboxylic ester group is also created at a slightly lower percentage of 3.6 ± 0.1% from the first dose, and remains at 4.6 ± 0.1% after the second dose.

Generally, the ion implantation process recoils hydrogen atoms at a rate higher than carbon and oxygen atoms from both the hydroxyl groups and the carbon backbone of the PVA molecules. We expected that C—O—C groups could be formed between two PVA chains as the cross-linker [10]. This is especially relevant to PVA as it belongs to a category of polymers favoring cross-linking [47] during the implantation process. We were not able to confirm this conclusion with our XPS data because the C—O—C binding energy overlaps with other peaks. A similar situation occurred for the C—N (amine) group with signals mixed in peaks H and B.

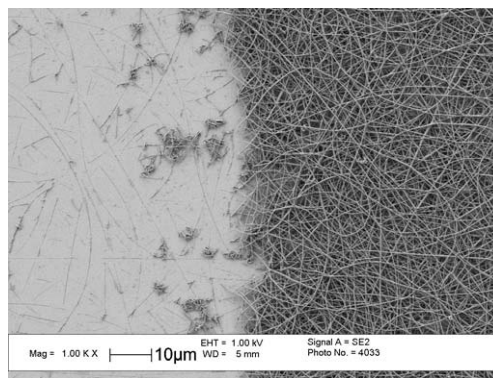
To confirm the introduction of cross-linking by the N<sup>+</sup> treatment, we conducted a solubility test on the PVA fibers pre- and post-treatment with 1.2 × 10<sup>16</sup> ions/cm<sup>2</sup> of N<sup>+</sup>. Fig. 5 shows an SEM image of the boundary area of the untreated (right side) and N<sup>+</sup> treated fibers (left side) after

**Table 1**

List of different chemical functional groups represented by the peaks labeled in XPS spectra at the corresponding binding energy shown in Fig. 4.

Peak	Functional groups	Binding energy (eV)
A	C—C*	285
B	C*—OH or C*—N or C—O—C* or C*—O—C=O	286.5
C	O—C*—O or N—C*—O	288
D	C—O—C*—O	289.1
E	C—O—H or C—O*—C or C—O—C=O*	532.7
F	O—C—O* or C—O*—C=O	533.5
G	N—C=O*	531.5
H	C—N* or N*—C=O	399.9

\* is designated to the source atom in the functional group.



**Fig. 5.** SEM image of the boundary area of the original (right side) and treated fibers (left side) after 10 min of soaking in water.

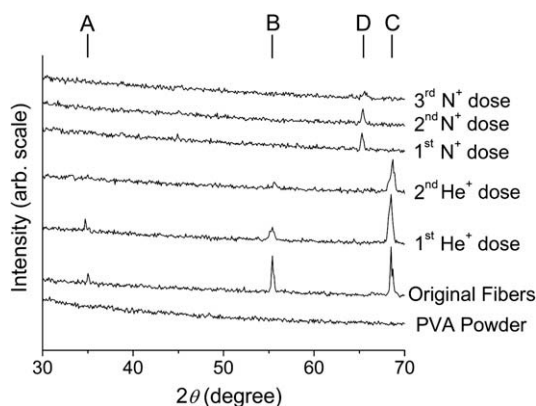


10 min of soaking in water. Only minor residue of the original fibers remained on the right side but most of the fibers dissolved. It can be seen that the untreated fibers produced from an aqueous solution is stabilized by cross-linking and are stable against dissolution when exposed to water.

Chemical modifications to the polymer chains occur in parallel to physical modifications during ion beam implantation. As the ion–polymer interaction induces an irreversible chain scission and cross-linking effect into the polymer matrix, new functional groups are created as free radicals temporarily increase the chemical reactivity. With the ion beam energy broadened with a Ta foil, the doping effect start at the surface of the fiber mat. Our XPS data showed that without the presence of nitrogen, as with  $\text{He}^+$  treatment, chemical modifications along the implantation path only generate new functional groups, such as carboxylic ester, from chain scission and cross-linking within PVA molecules. Although this has been shown to alter cell adhesion on polypropylene and polytetrafluoroethylene [21], these materials have chemical compositions very different from PVA, which generates different types of functional groups. Doping with  $\text{N}^+$  generates amine and amide functional groups. As cell adhesion is found to improve with the introduction of such groups at the surface of polymeric materials [22,48], this  $\text{N}^+$  treatment technique may be useful for improving cell compatibility on the treated PVA fiber surface.

### 3.6. Effect of ion beam treatment on crystalline structure

After  $\text{He}^+$  and  $\text{N}^+$  treatment, the fiber mats were analyzed by XRD techniques to determine their crystalline structure. Fig. 6 shows the XRD spectra of electrospun PVA fibers before and after various stages of the two different ion beam treatments for regions of  $30^\circ < 2\theta < 70^\circ$ . The figure also includes a comparison to PVA powder. The PVA fibers show some degree of crystalline structure relative to the PVA powder, with one weak Bragg peak (A) at  $2\theta = 35^\circ$ , one medium peak (B) at  $55.4^\circ$  and one intense reflection peak (C) at  $68.5^\circ$ . The crystalline structure of



**Fig. 6.** XRD spectra (with four  $2\theta$  indexes at the top) of PVA powder, original electrospun PVA fiber mats, two dose steps of helium ion beam treatment and three dose steps of nitrogen ion beam treatment applied to the PVA fiber mats (offset for clarity).

the original fibers provides a baseline for studying the effect of ion beam implantation.

The first dose of  $\text{He}^+$  treatment showed a deterioration of the original crystalline structure at the peak (B) at  $55.4^\circ$  and a broadened peak (C) at  $68.5^\circ$ , which is consistent with the weakening of elastic modulus observed with AFM. The second dose of  $\text{He}^+$  treatment showed a further deterioration of crystallinity (with the peak (A) at  $35^\circ$  disappearing along with a continued drop in intensity at the other two  $2\theta$  values). On the other hand, during  $\text{N}^+$  treatment, the deposition energy is significantly higher than for  $\text{He}^+$  to achieve an identical doping depth profile. As shown in Fig. 5, after the first dose of treatment the original crystalline structure of the fiber completely disappeared and a new peak (D) is seen at  $2\theta = 65.4^\circ$ . This can explain the overall 30% increment on the elastic modulus of the fibers. The XRD spectrum after the second  $\text{N}^+$  dose was almost identical. This is consistent with the results of AFM mechanical testing on the fibers, which showed no significant weakening. The last  $\text{N}^+$  dose caused the intensity of the new peak to drop by more than 50% which is similar to the trend of average elastic modulus to decrease about 50% of the value of the first  $\text{N}^+$  dose.

## 4. Conclusions

We developed simple procedures to make use of ion implantation with a broad energy range ion beam as a post-processing treatment technique to modify the elastic modulus as well as the chemical structure of electrospun PVA fibers without damaging the surface morphological features.

We confirmed that the macroscopic-scale stiffening effect occurs in nano-sized electrospun fibers, using an AFM study with multi-point mechanical bending tests performed on individual fiber before and after ion beam treatment. With a treatment of  $8.0 \times 10^{15}$  ions/cm<sup>2</sup> of  $\text{N}^+$ , we observed a 30% increase in the elastic modulus. Meanwhile, the fiber diameter decreased by up to 11%. Two additional  $\text{N}^+$  treatments with the same dose showed that the improvement in the elastic modulus is dosage dependent. At the same time, key chemical modifications were achieved with the introduction of amine and amide functional groups using  $\text{N}^+$  beam which could improve cell compatibility of PVA fibers. Treatment by  $\text{He}^+$  with a dose of  $8.0 \times 10^{15}$  ions/cm<sup>2</sup>, on the other hand, showed the opposite trend, with a degradation of 63% in elastic modulus and no significant change in fiber diameter.

The approach developed is generally applicable to electrospun polymer fibers for control of their mechanical properties and chemical modification for cell compatibility.

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